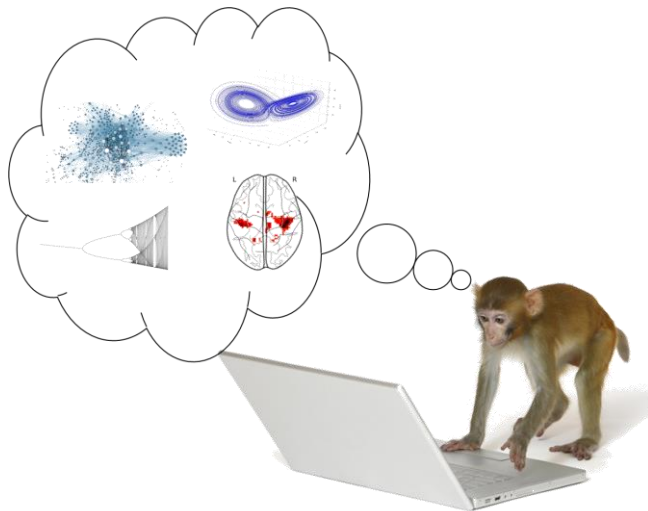
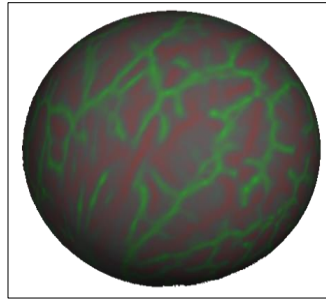
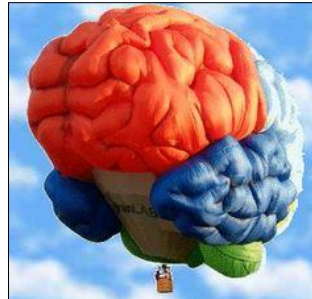




Introduction to Neuroimaging

for Algebraic Topologists



Dr. John D. Griffiths

Rotman Research Institute

Baycrest, Toronto



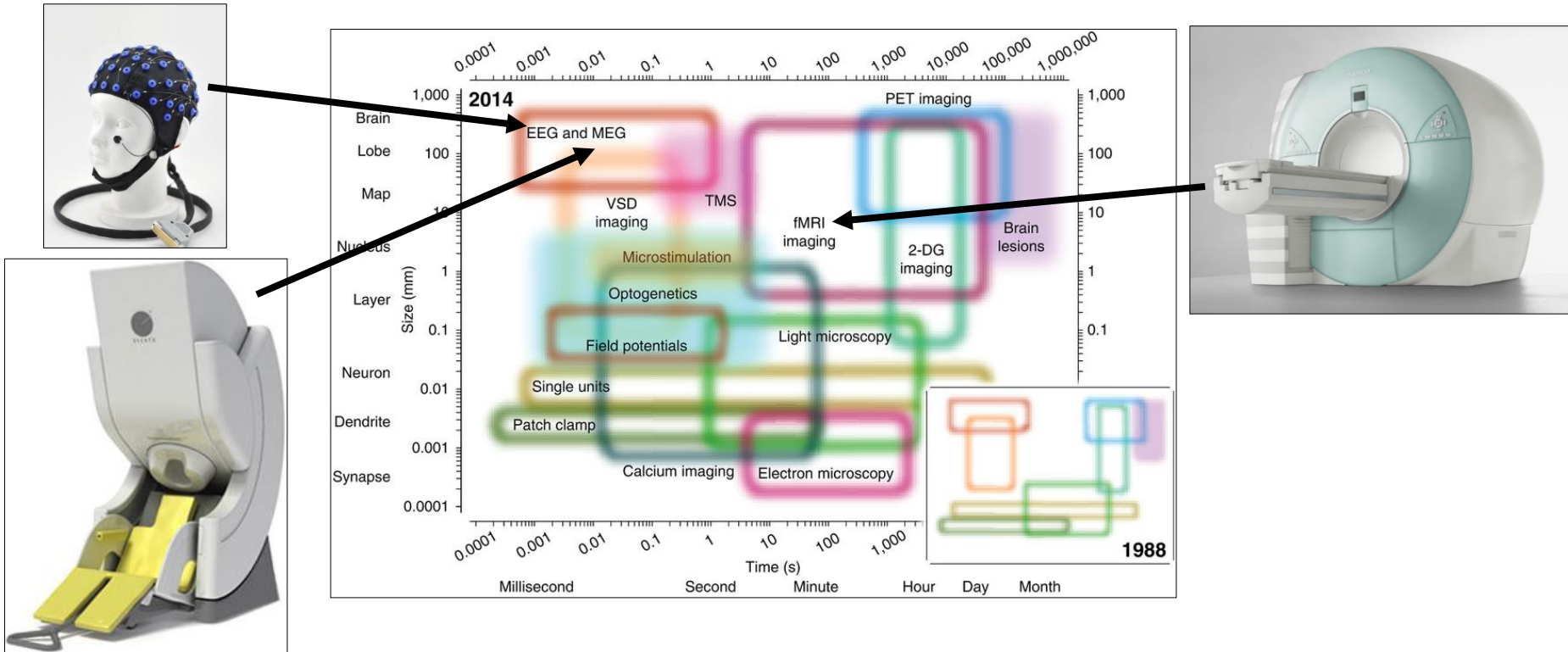


Overview

- Structural MRI
 - Modalities & Contrasts
 - Macro-neuroanatomy
 - Registration
 - Parcellations
 - DWI Tractography
- fMRI
 - Origins of the BOLD signal
 - Experimental Paradigms
- M/EEG
 - Origins of the M/EEG signal
 - Source localization
- Connectivity
 - The three Cs
 - Connectomics
 - Neural mass modelling

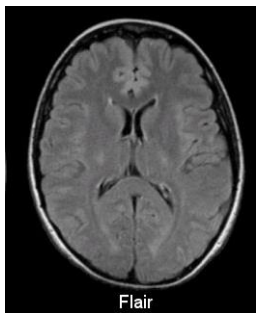
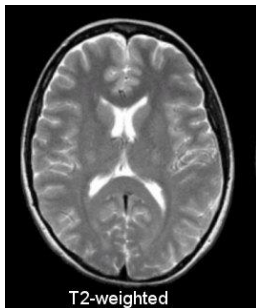
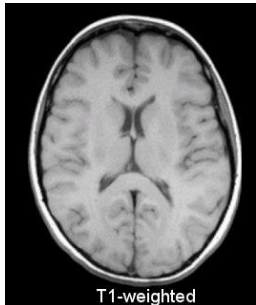


Tools of the trade



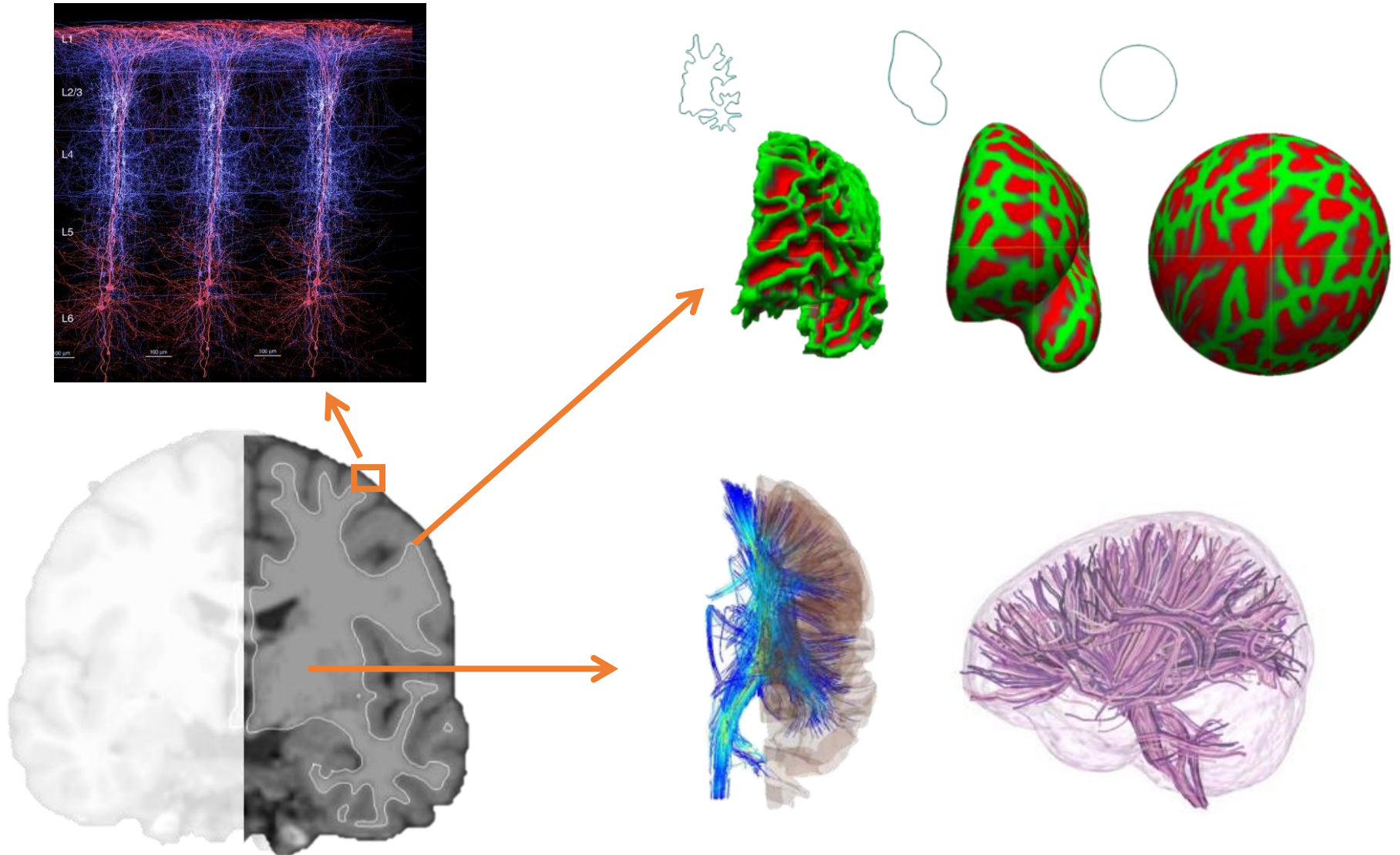


Imaging Brain Structure



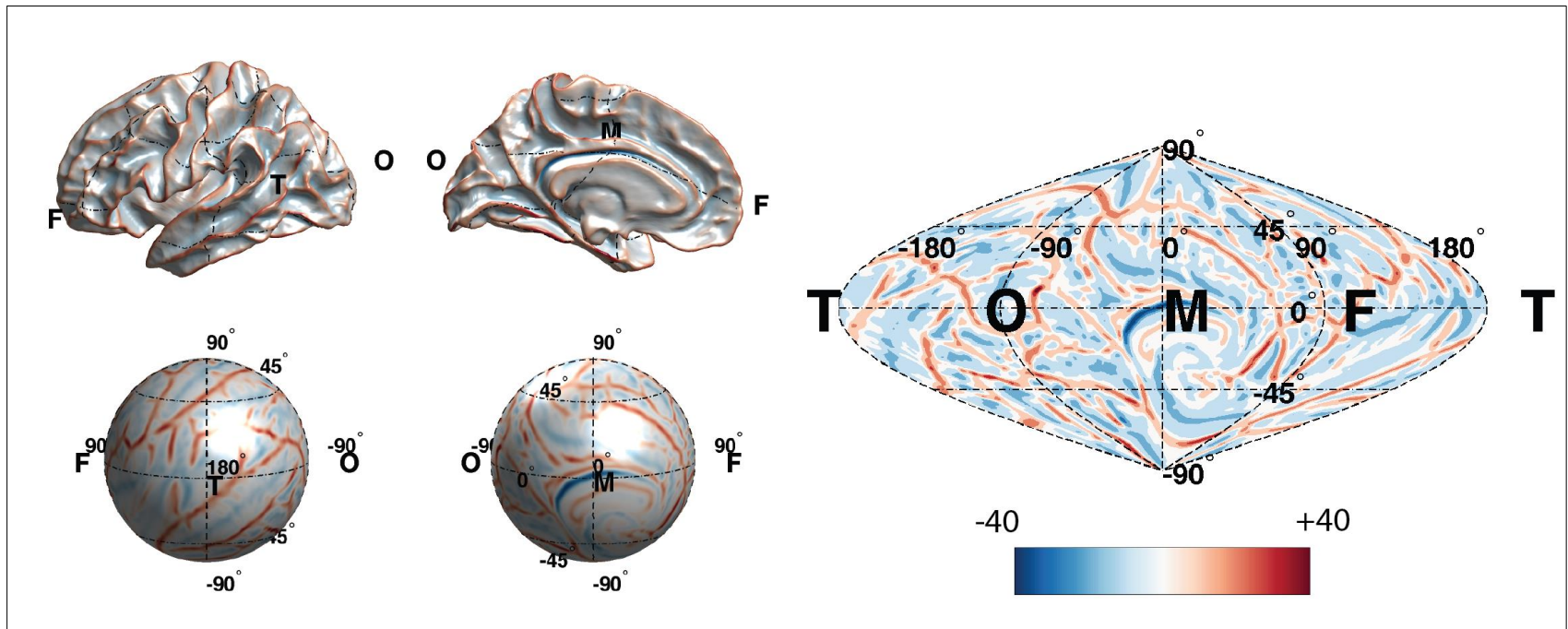


Macroscopic Cortical Anatomy





Spherical topology of cerebral hemispheres



Robinson et al. 2016

(see also: <http://gallantlab.org/brainviewer/sulcigyri/>)



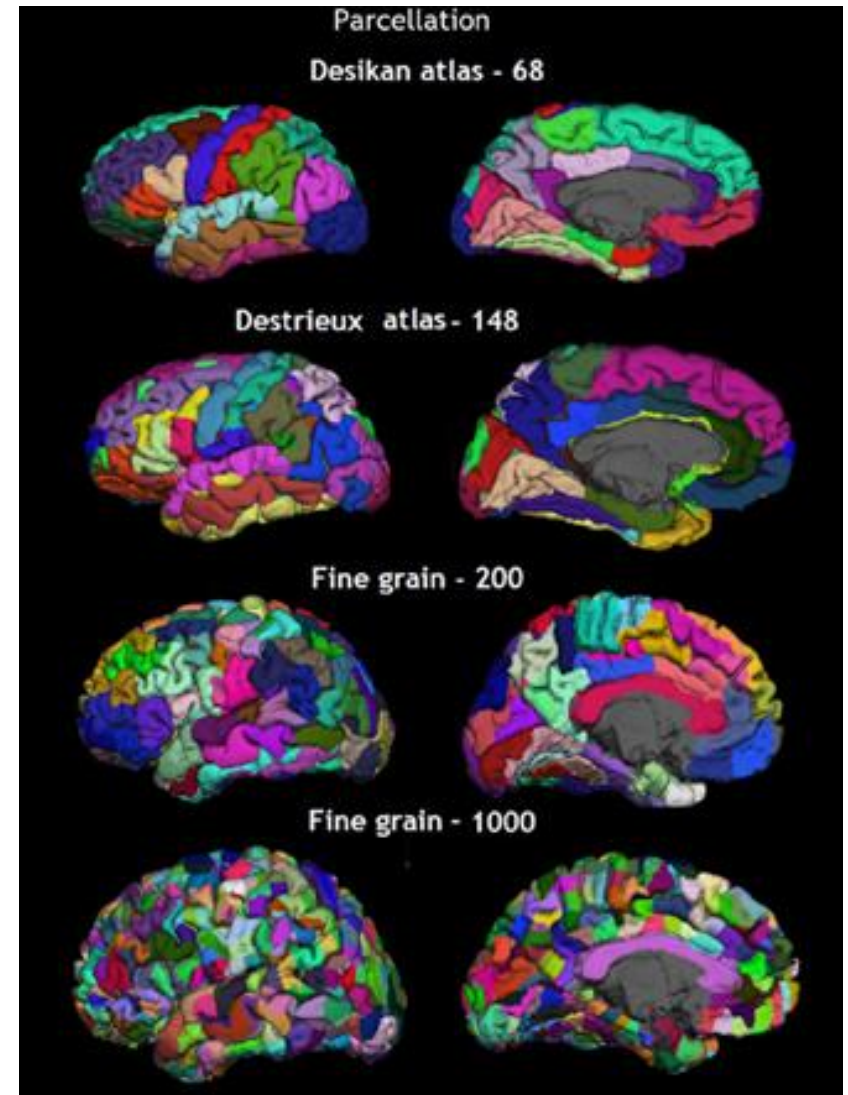
Parcellations

Can be thought of as
neuroanatomically principled
form of data downsampling

Quite a few around...

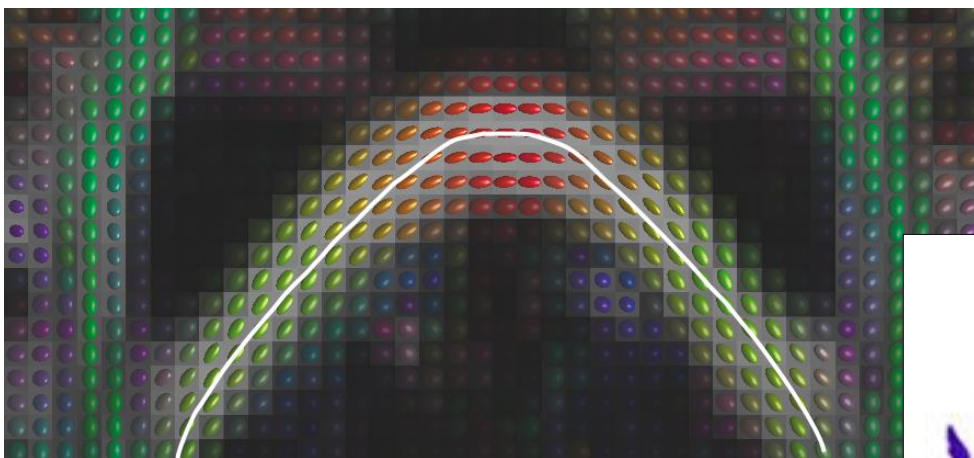
Bit of a wild west...

Rapidly evolving field





Tractography





Origin of the BOLD signal

Blood oxygenation-level-dependent (BOLD) signal:

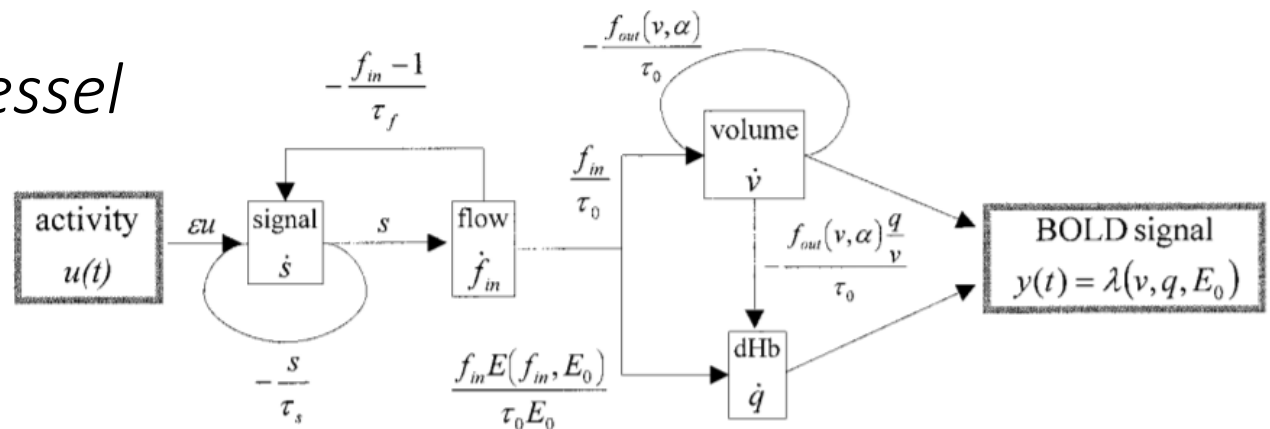
Neural activity -> increased oxygen consumption

-> increased blood flow

-> change in magnetic susceptibility

'Balloon-Windkessel

Model':





Experimental & Statistical Paradigms

'Classical' mass-univariate analysis

HRF-convolved boxcar regressor

-> beta -statistic images for each contrast

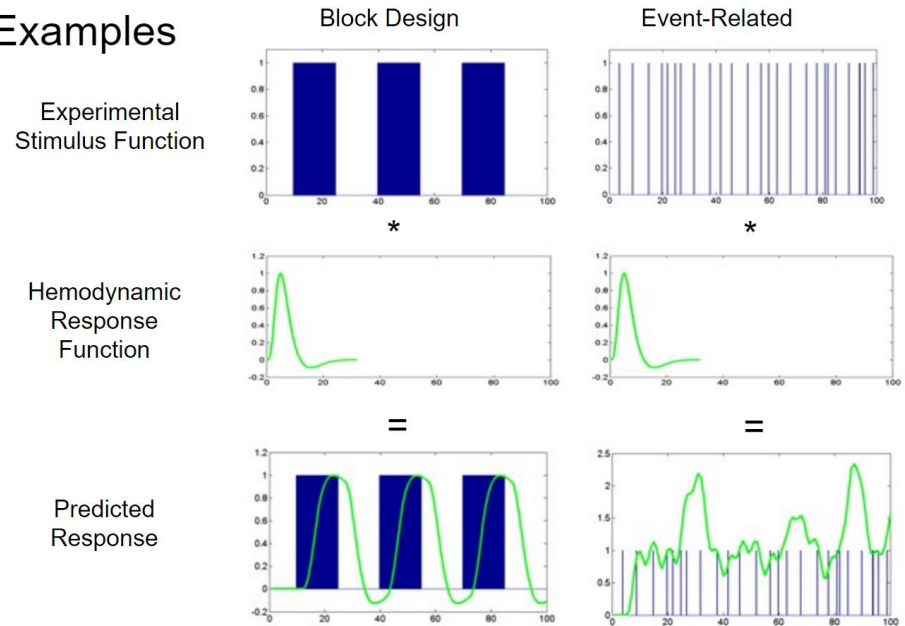
first-level mass-univariate analysis

-> t/F statistic images for each subject

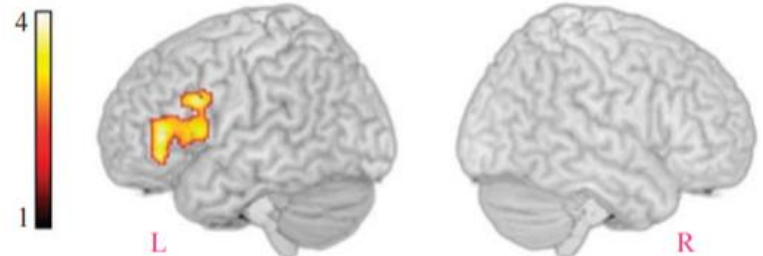
Enter into second-level (group) analysis

-> 'activation maps'

Convolution Examples



Words > Non-words





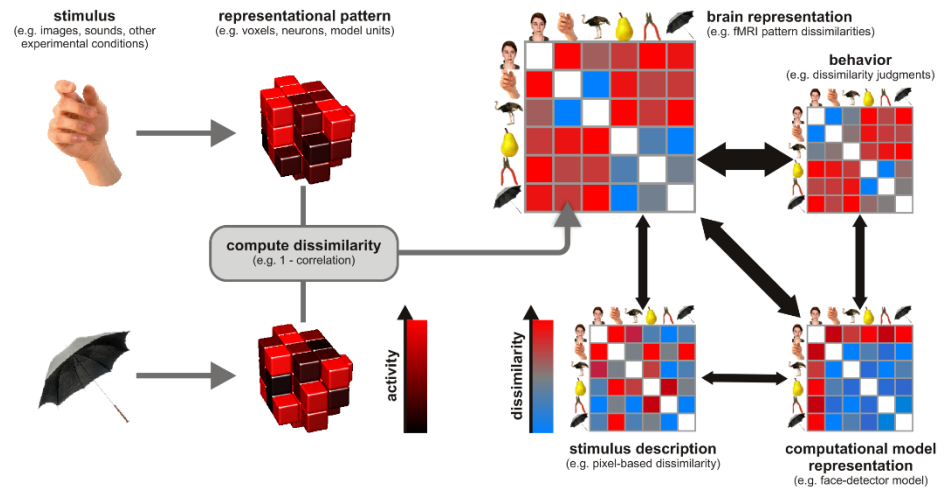
Experimental & Statistical Paradigms

Multi-voxel pattern analysis

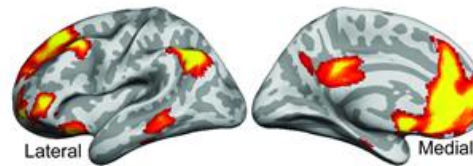
HRF-convolved boxcar regressor

-> beta + t/F -statistic images for each contrast, for each subject

multivariate analysis on patches of voxels

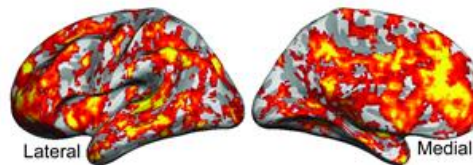


A. GLM



Kievit & Kiregeskorte 2013

B. MVPA





Experimental & Statistical Paradigms

Resting State

What?

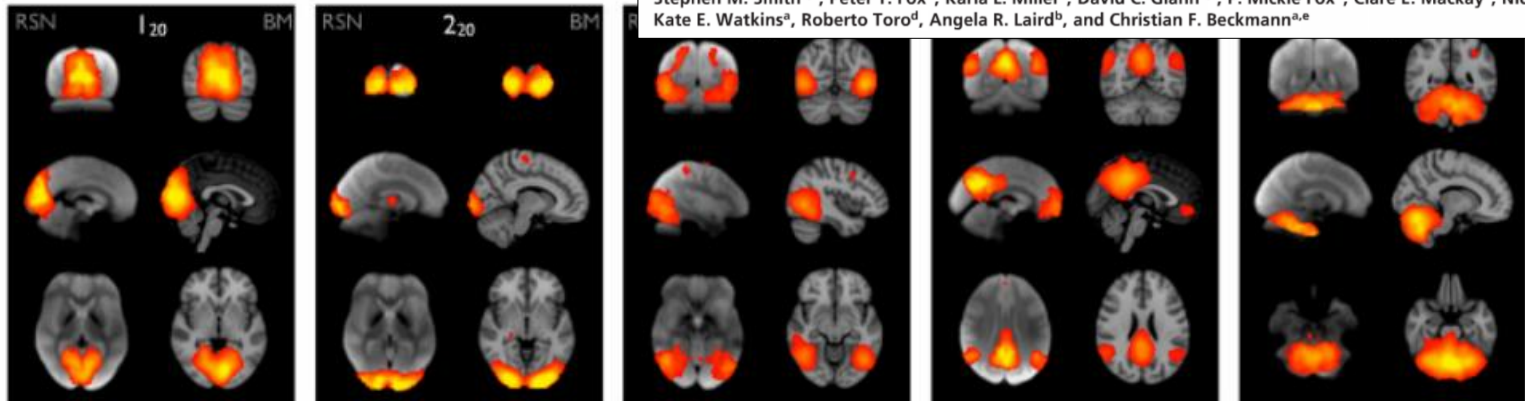
1. An experimental paradigm (barely) for measuring brain activity at rest
2. What the brain is doing at rest
3. Specific, canonical patterns of coherent low-frequency fluctuations. At rest.
 - > 'RSNs'

Why?

- Flexible, easy, practical...etc..
- *Links to neurocognitive structures*

Correspondence of the brain's functional architecture during activation and rest

Stephen M. Smith^{a,1}, Peter T. Fox^b, Karla L. Miller^a, David C. Glahn^{b,c}, P. Mickle Fox^b, Clare E. Mackay^a, Nicola Filippini^a, Kate E. Watkins^a, Roberto Toro^d, Angela R. Laird^b, and Christian F. Beckmann^{a,e}





Qs?

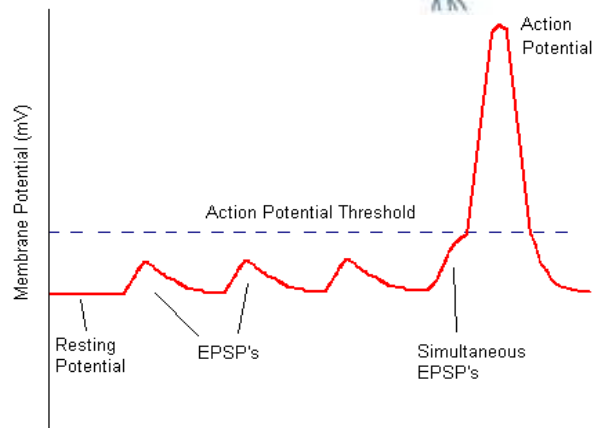
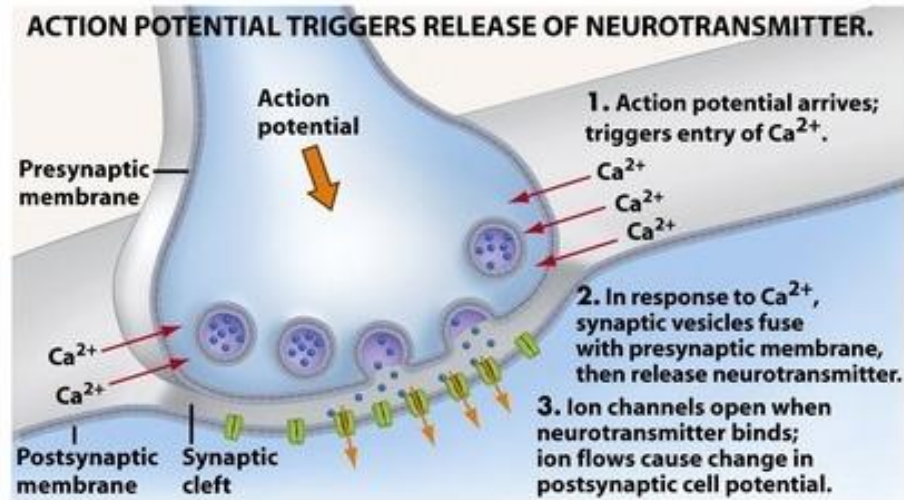
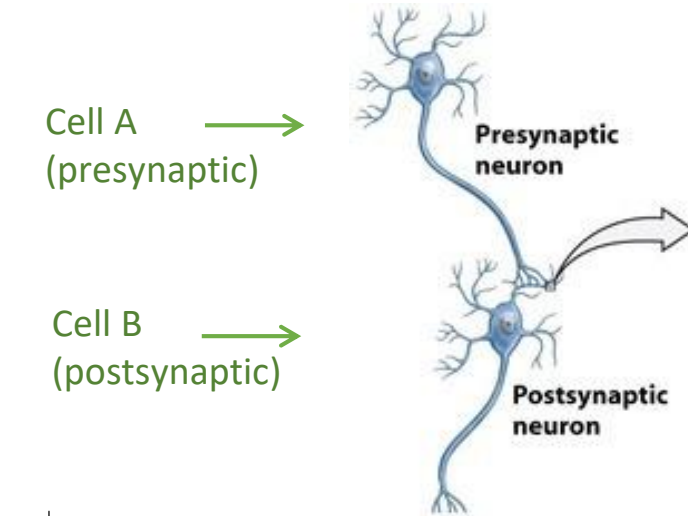


**KEEP
CALM
AND
ASK
QUESTIONS**



Physiological Basis of M/EEG signals

1. Action Potentials and post-synaptic potentials

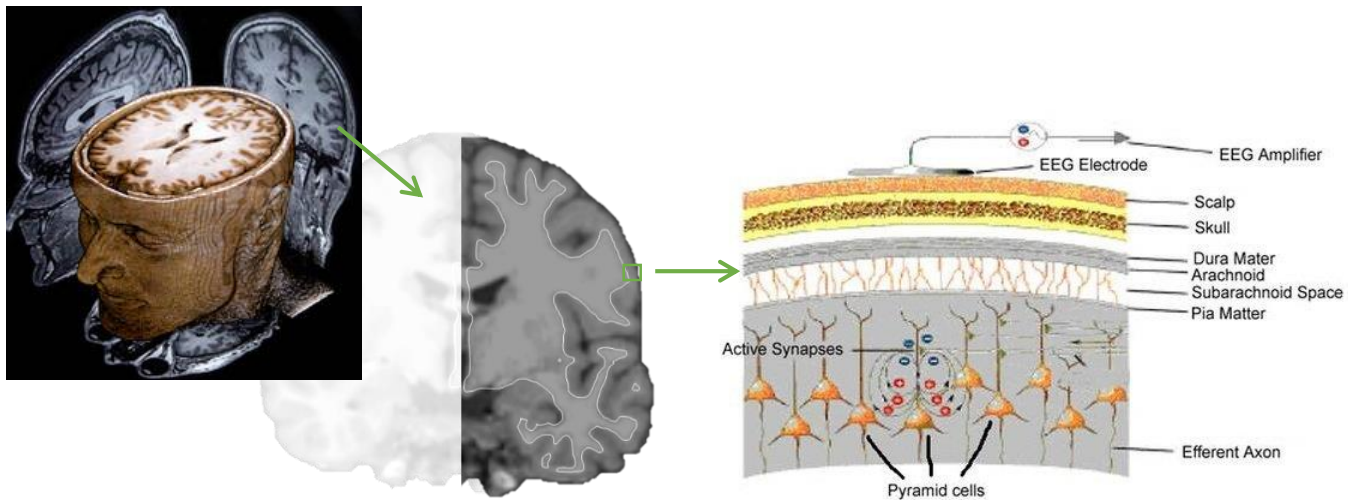


- Cell A fires
 - Action potential travels along axon of cell A
 - Cell A releases neurotransmitter (generally)
 - EPSP / IPSP at dendritic / somatic membrane of cell B
- = micro-current source & origin of EEG signal



Physiological Basis of M/EEG signals

2. Apical dendrites in the cortical ribbon

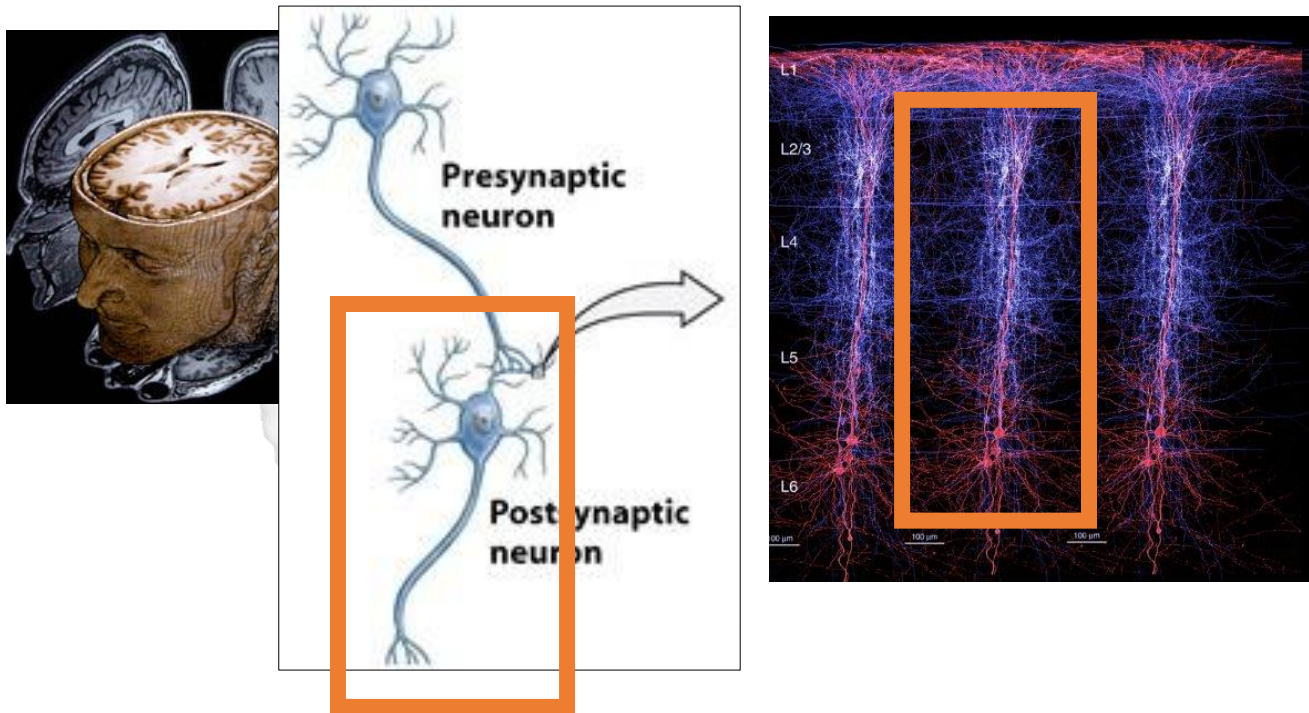


Synchronized micro-current sources due to PSPs in aligned apical dendrites of cortical pyramidal cells summate to produce meso-current sources



Physiological Basis of M/EEG signals

2. Apical dendrites in the cortical ribbon

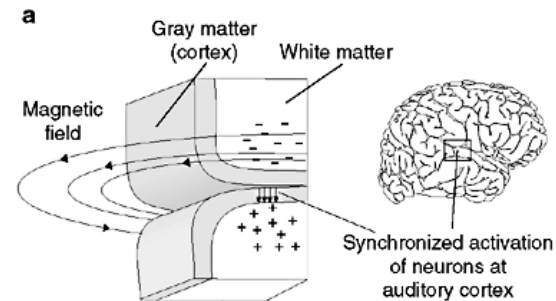
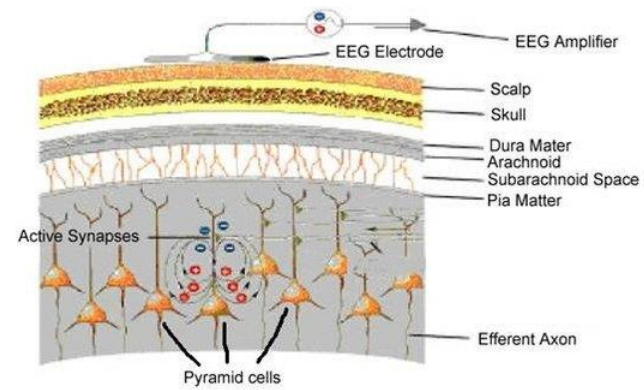
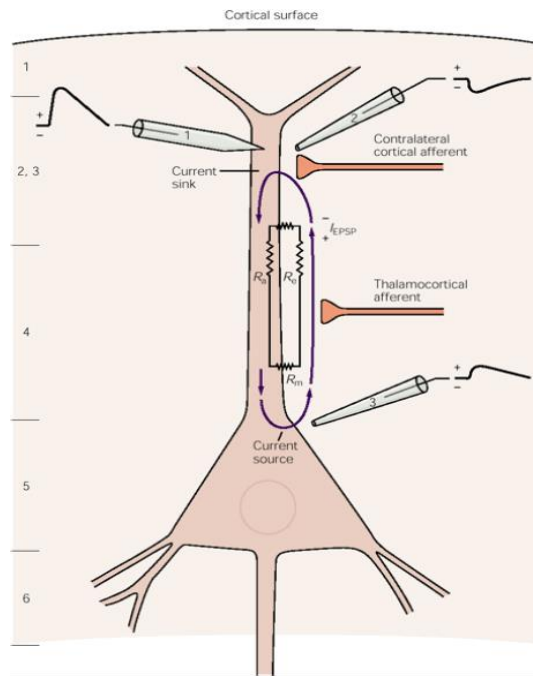


Synchronized micro-current sources due to PSPs in aligned apical dendrites of cortical pyramidal cells summate to produce meso-current sources



Physiological Basis of M/EEG signals

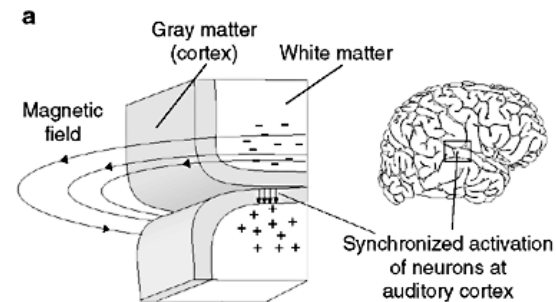
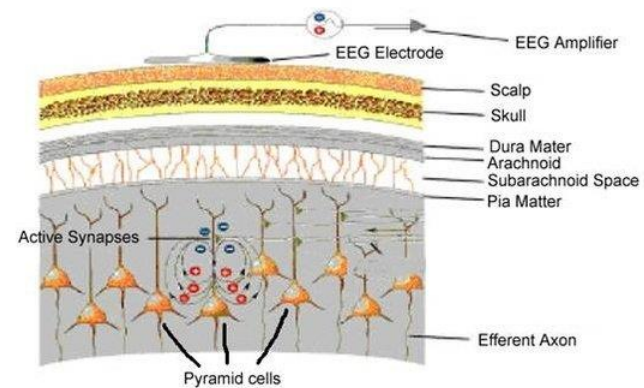
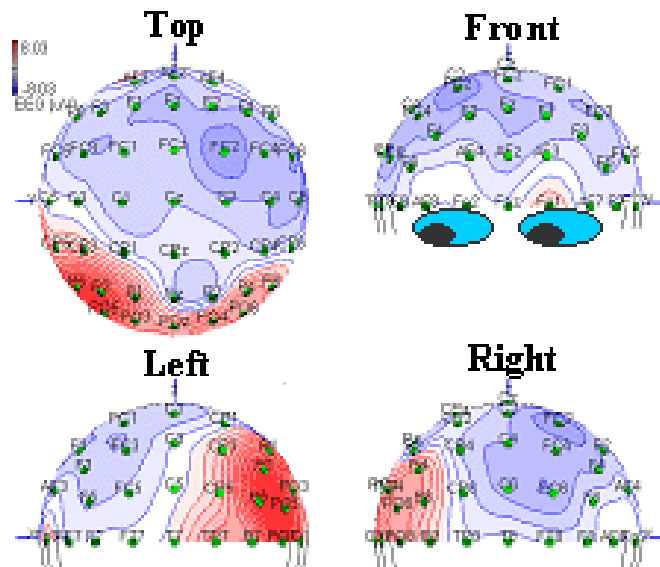
3. Micro- and meso-current sources





Physiological Basis of M/EEG signals

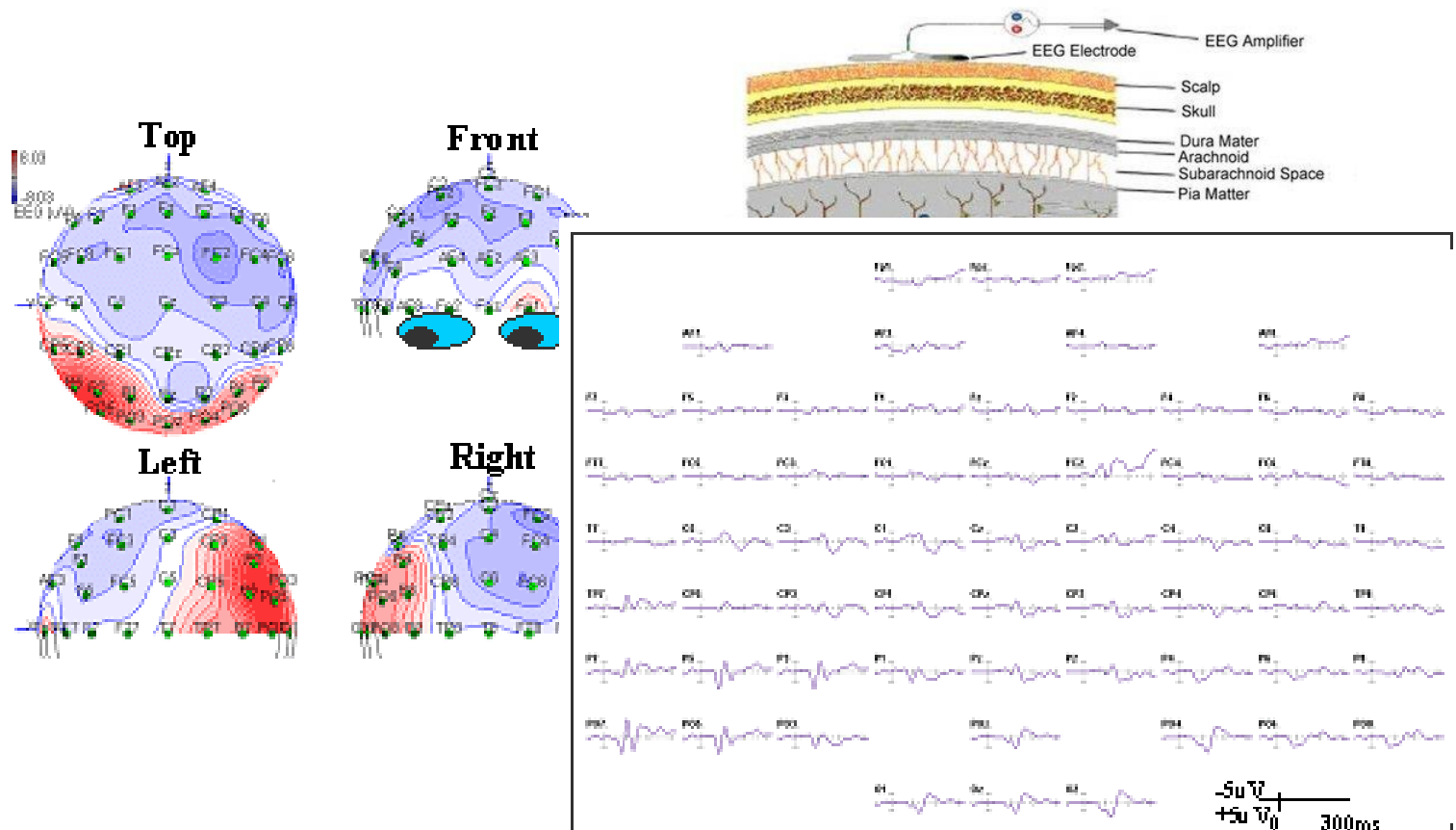
4. *Electrical/magnetic field distribution on the scalp*





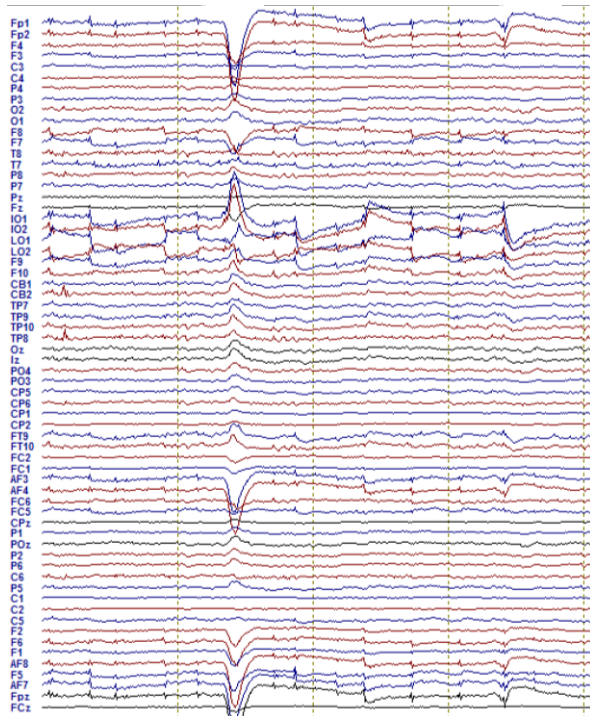
Physiological Basis of M/EEG signals

4. *Electrical/magnetic field distribution on the scalp*

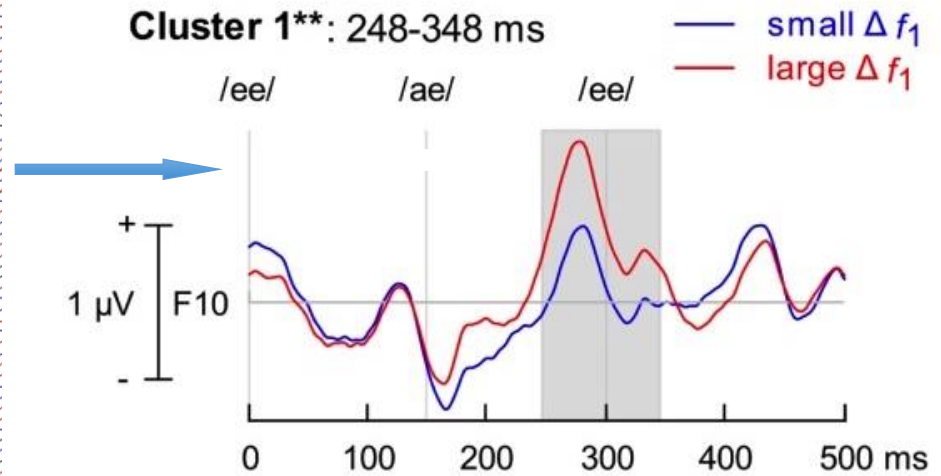




Event-related potentials (ERPs)

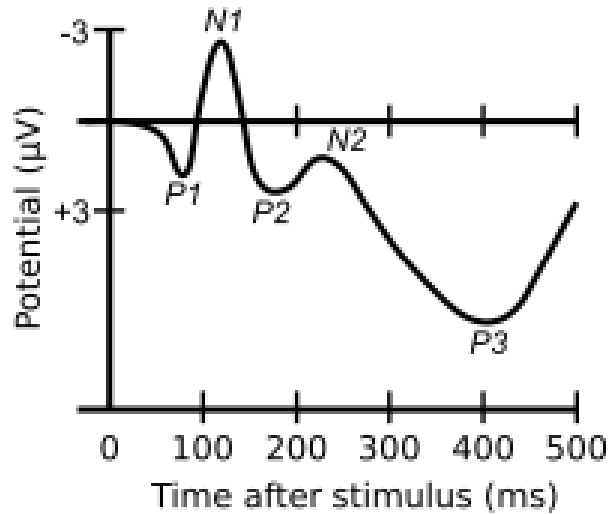


Grand average waves





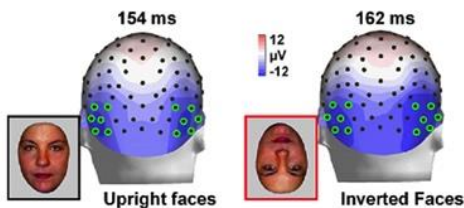
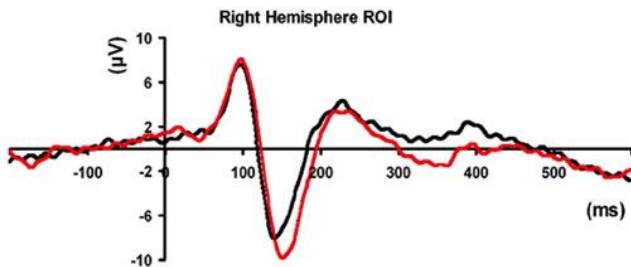
Event-related potentials (ERPs)



Main components:
N1, P2, MMN, N2b, N2pc, P300 (P3a, P3b), N400, P600

Main classification:
exogenous/endogeneous

Component magnitudes + latencies
are modulated by cognitive
manipulations

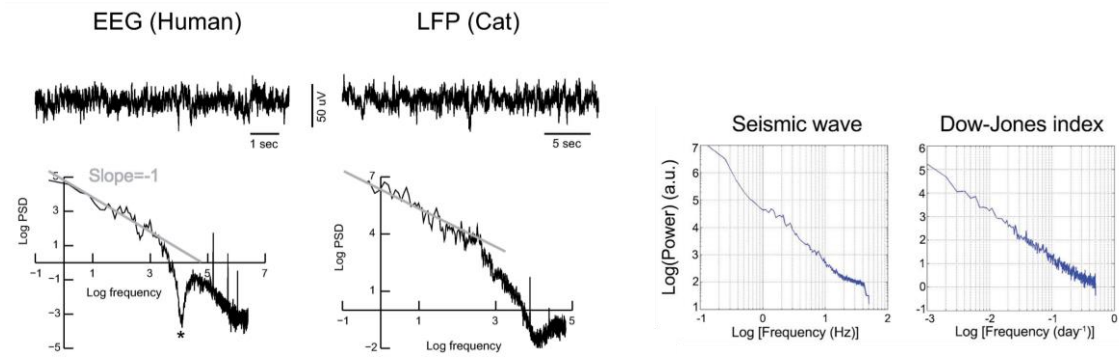




Frequency & time-frequency analysis

Power law scaling

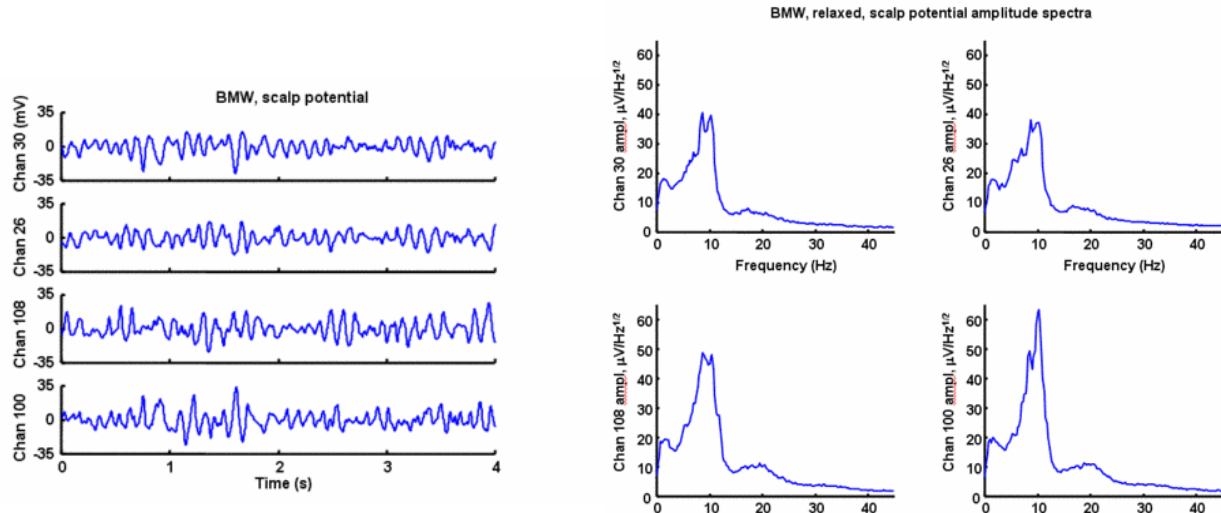
- log power is a linear function of log frequency with some exponent α



Bedard et al. 2016; He et al. 2010

Alpha rhythm

- (by far) most dominant spectral feature of EEG
- Slows with age
- Multiple spatial components



Nunez et al. 2006



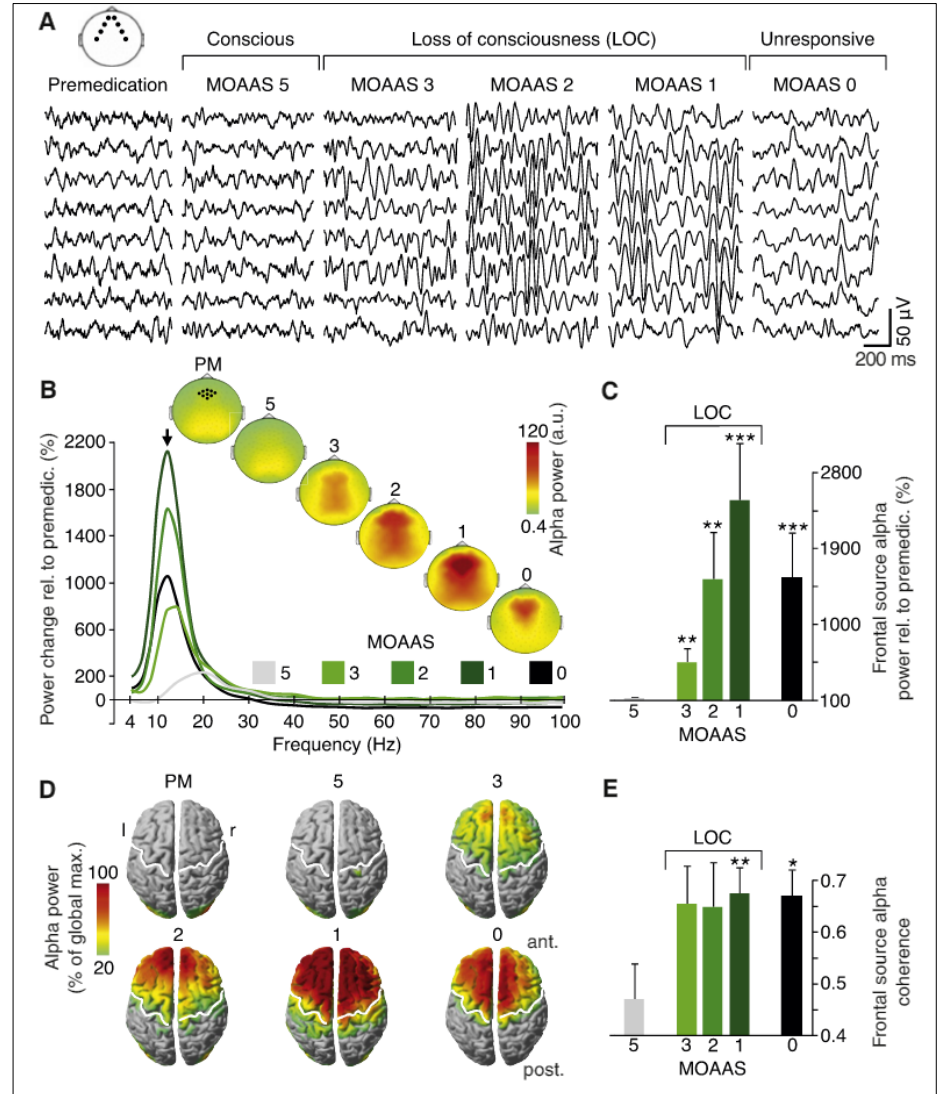
Frequency & time-frequency analysis

Power law scaling

- log power is a linear function of log frequency with some exponent α

Alpha rhythm

- (by far) most dominant spectral feature of EEG
- Slows with age
- Multiple spatial components





Multi-scale entropy

Sample entropy:

“Negative logarithm of the probability that if two sets of simultaneous data points of length m have distance $< r$ then two sets of simultaneous data points of length $m+1$ also have distance $< r$ ”

$$SE = -\log (A/B)$$

where

A = # of length $m+1$ pairs with difference $< r$

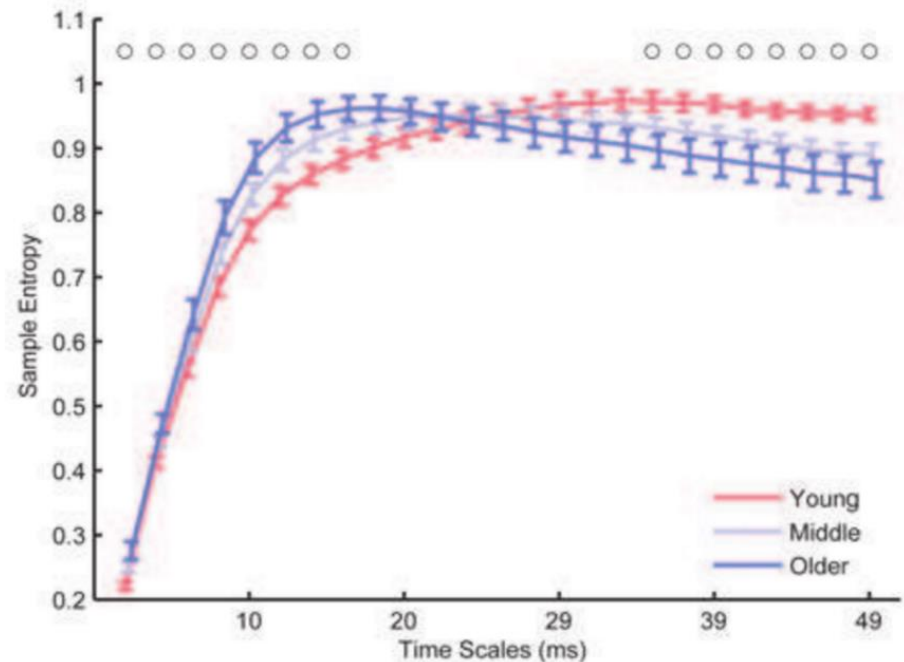
B = # of length m pairs with difference $< r$

Measure of *regularity* or *complexity*

Multiscale entropy:

sample entropy for multiple levels of downsampling

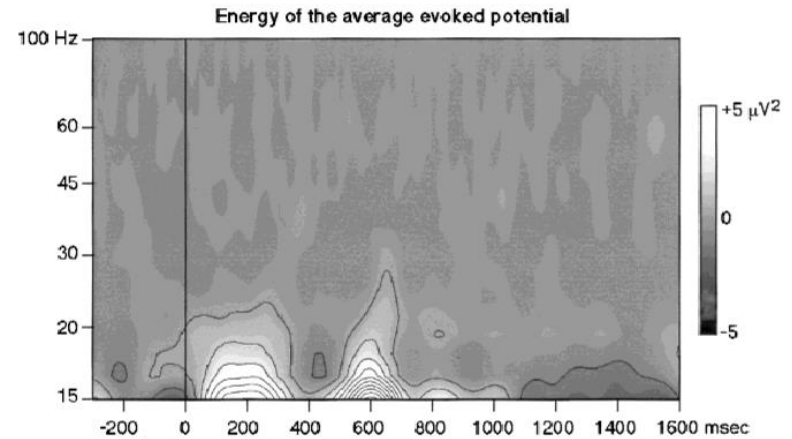
changes with age, development, cognitive state



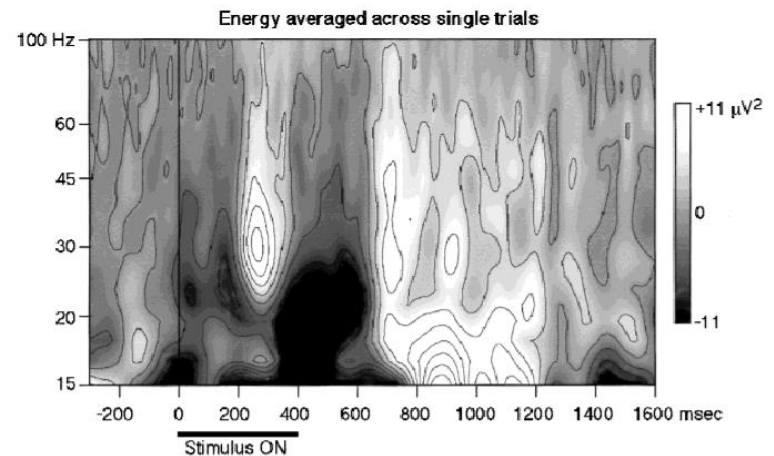


Evoked vs. Induced Responses

Evoked power:
average > TF decomposition



Induced power:
TF decomposition > average



M/EEG Source Analysis

Problems and strategies

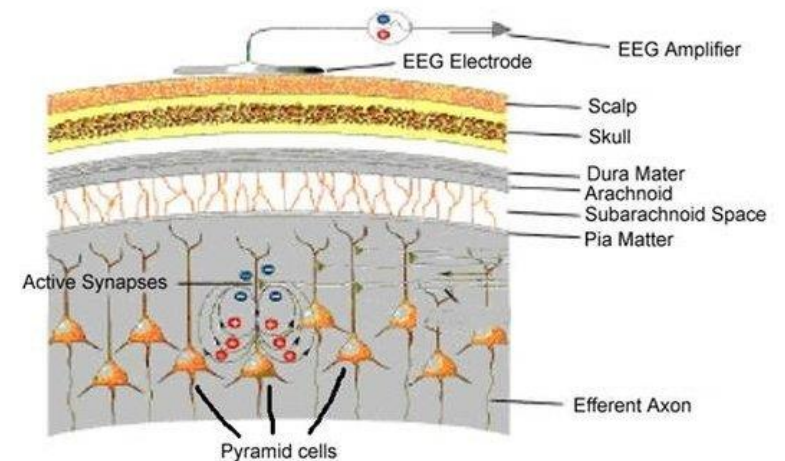
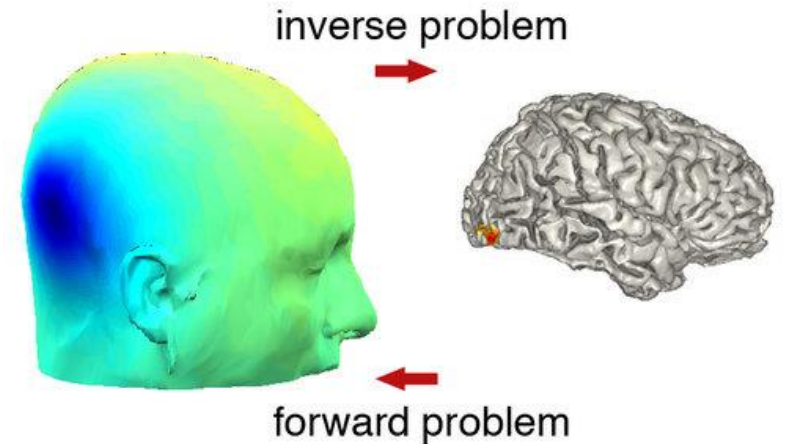
Inverse problem is ill-posed; requires constraints

Three families of approaches:

- Focal dipole modeling
- 'Scanning' / spatial filters
- Distributed source modelling

Main source of error: registration

EEG data requires more detailed tissue conductivity models than MEG





M/EEG Source Analysis

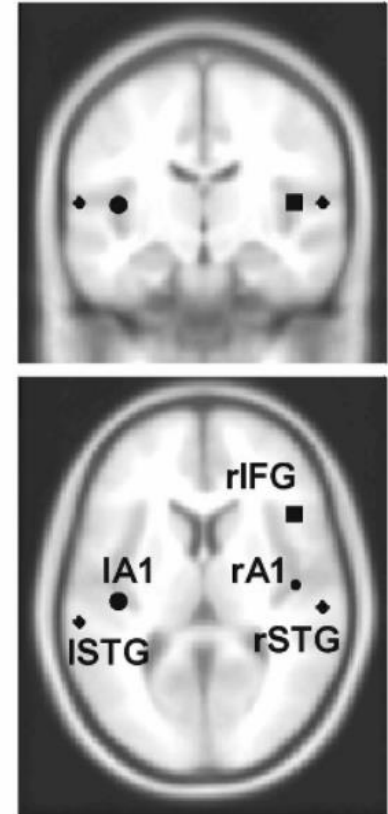
Dipole Modelling

5 parameters (per dipole):
 position (x,y,z)
 orientation (theta,phi)

Incrementally add in until best fit / most parsimonious fit

Not always 100% automated (v. nonlinear optimization problem)

Not recommended....



M/EEG Source Analysis

Beamforming

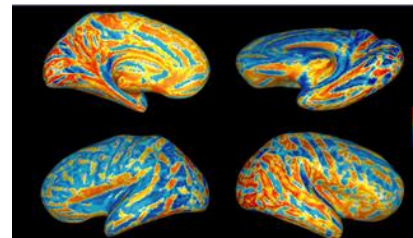
spatial filter, optimized independently for every source location

not an inverse solution

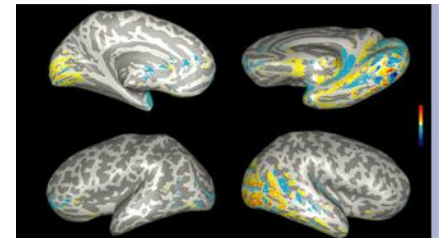
SAM: scalar, nonlinear; find dipole orientations that maximize total power/noise ratio

LCMV: vector, linear; maximize variance subject to unity gain constraint

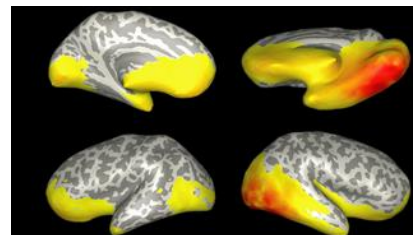
(not generally used in EEG...)



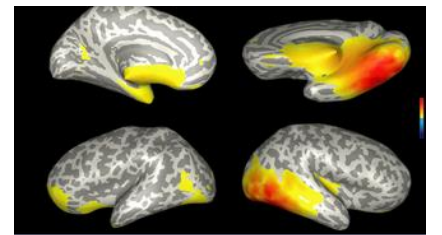
Match Filter



ACB



LCMV



SAM



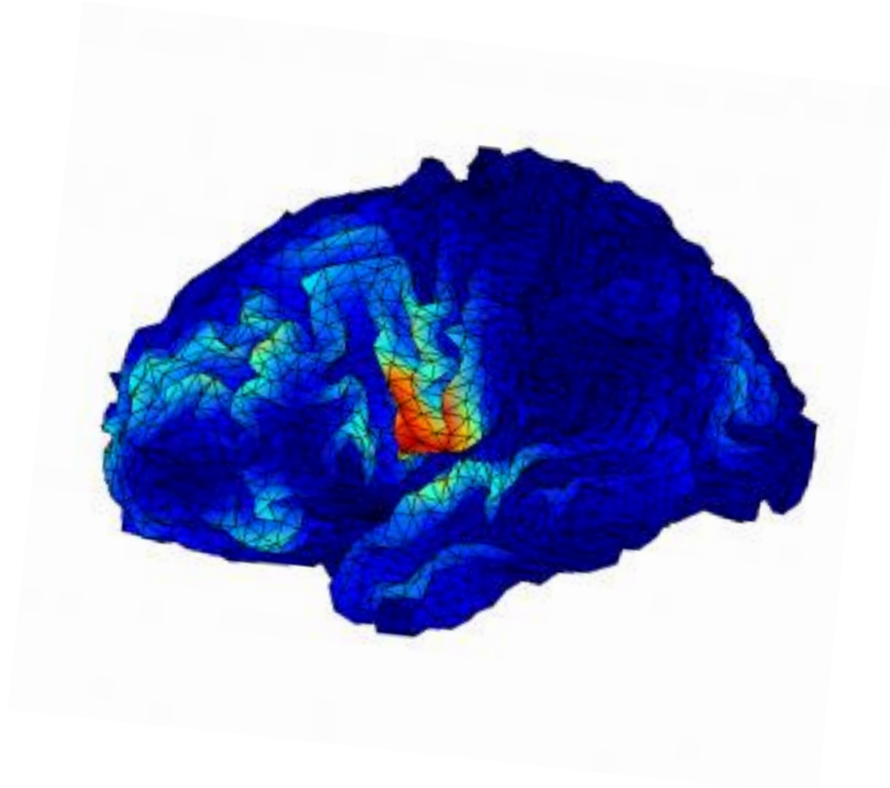
M/EEG Source Analysis

Distributed Inverse Source Models

Assumed fixed dipole orientations from cortical surface

-> linear, underdetermined system of eqs $\mathbf{B} = \mathbf{LJ} + \mathbf{E}$

Algorithms differ in regularization, depth-weighting, priors on source locations, sparsity



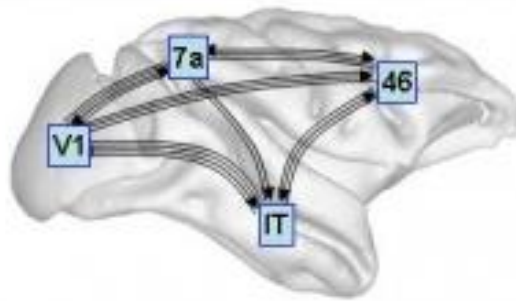


Connectivity & Networks

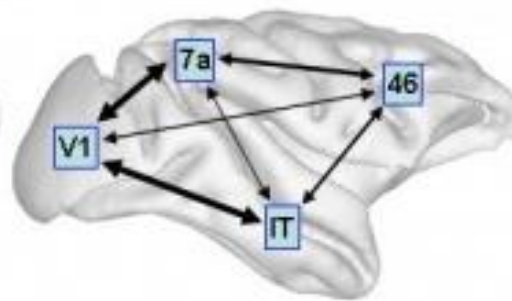


The three C's

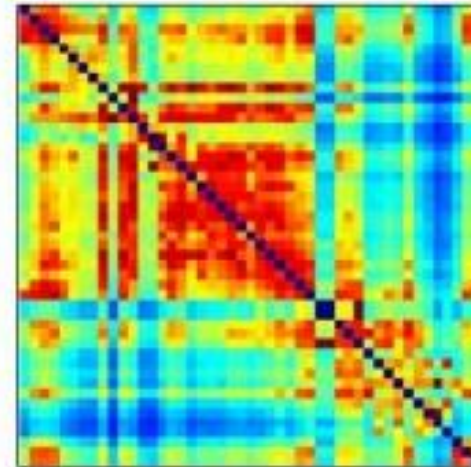
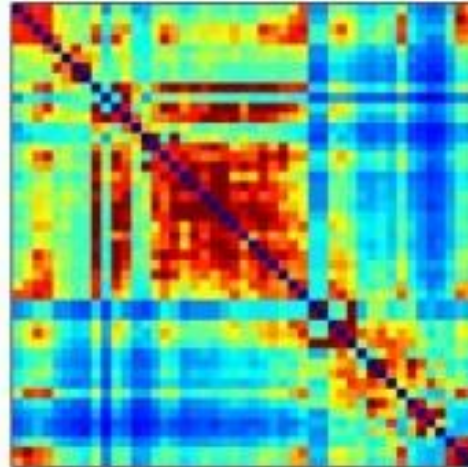
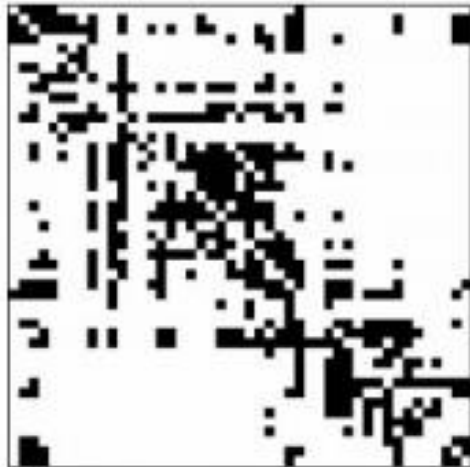
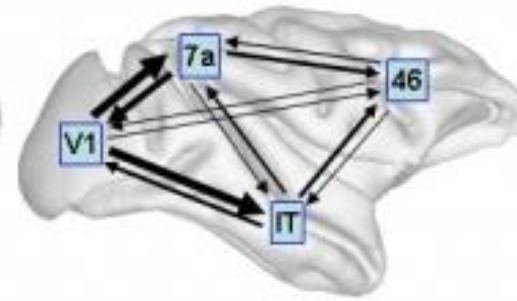
structural connectivity



functional connectivity



effective connectivity





Functional/Effective Connectivity

Metrics of choice

fMRI

- Pearson Correlation
- Partial Correlation
- Wavelet coherence
- ICA

M/EEG

- Imaginary Coherence
- Phase synchrony
- Bi/Multivariate Time/Freq domain Granger Causality
- Band-limited power correlations



Connectomics

Connectome

From Wikipedia, the free encyclopedia

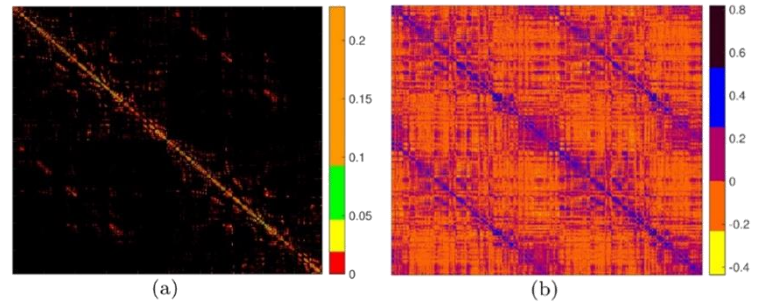
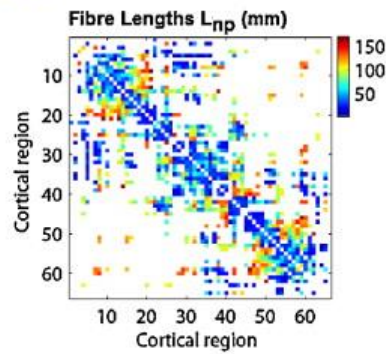
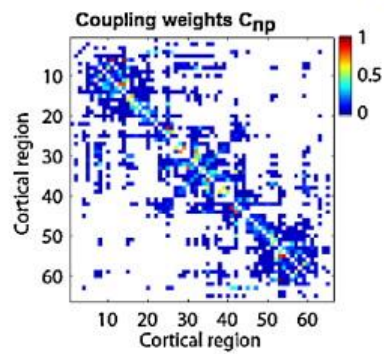
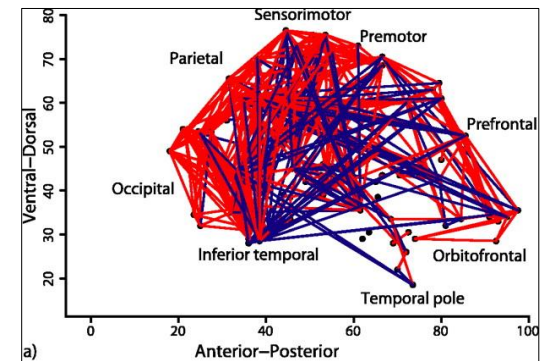
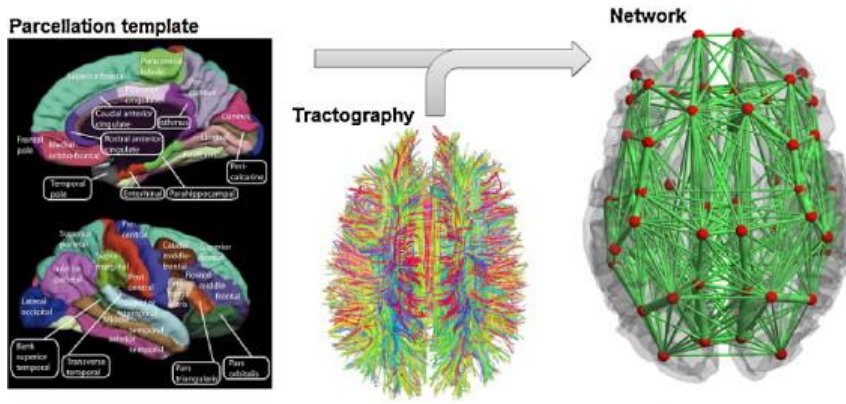
A **connectome** ([/kəˈnɛktəʊm/](#)) is a comprehensive map of **neural connections** in the **brain**, and may be thought of as its "**wiring diagram**". More broadly, a connectome would include the mapping of all neural connections within an **organism's nervous system**.



Connectomics

Structural connectome

Functional connectome

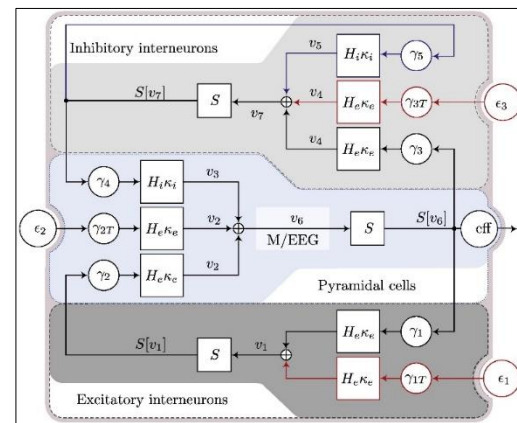
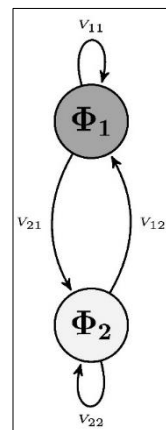
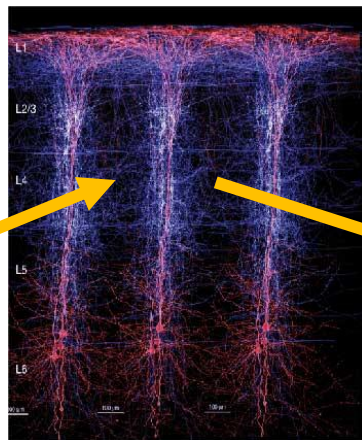
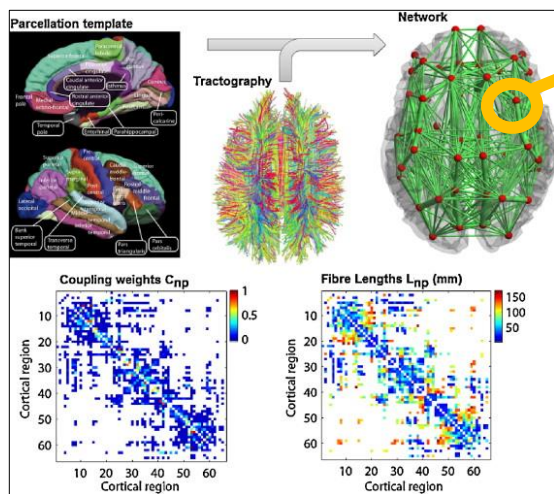


Daducci et al. 2012

Achard et al. 2006



Modelling neuroimaging data with networks of neural masses





Conclusions

High-resolution structural MRI data used for spatial alignment and identification of where to sample from (e.g. grey matter ribbon)

fMRI: = good spatial, poor temporal resolution

M/EEG = variable spatial; excellent temporal resolution

In practice, generally, we/you are likely to be working with parcellation / ROI time series

-> changes spatial resolution

Macro-connectomics approach: construct whole-brain networks from:

a) synchronization/correlation of ROI time series

-> 'functional connectome'

b) strength of anatomical connections

-> 'structural connectome'



That's a wrap 😊



Modelling rsfMRI non-stationary covariance-structure

